

Stress and Disorder in a Confluent Epithelium

Inferring tissue mechanics from geometry

Alexander Nestor-Bergmann

University of Cambridge

Outline

Introduction

- Understanding Forces in Morphogenesis
- Vertex modelling

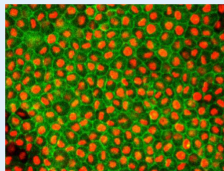
Mechanical modelling

- Cell-level stress
- Tissue-level stress

Anisotropic Elasticity

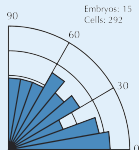
- Small-on-large deformations
- Elastic Moduli for Isotropic Tissues

The Biological Question



Control Cells

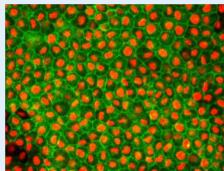
Randomly oriented on average



Division Angles

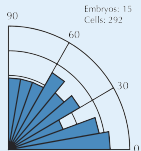
Uniformly distributed

The Biological Question



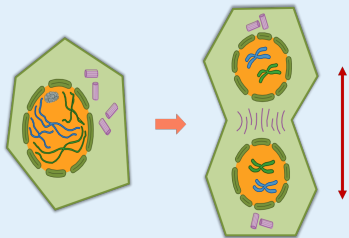
Control Cells

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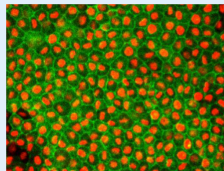


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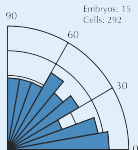


The Biological Question



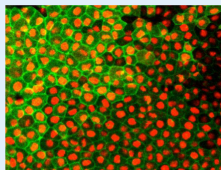
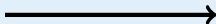
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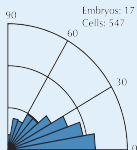
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Stretched Cells

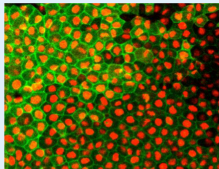
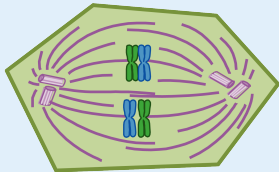
Aligned with direction of stretch



Division Angles

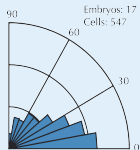
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The Biological Question



Stretched Cells

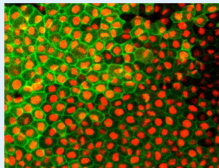
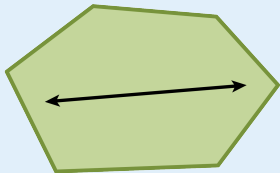
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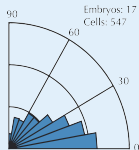
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The Biological Question



Stretched Cells

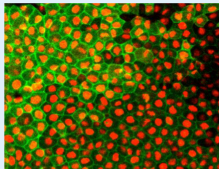
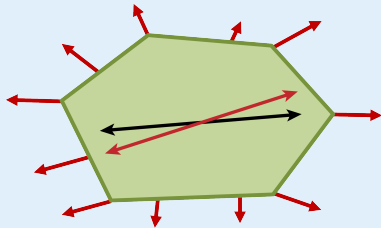
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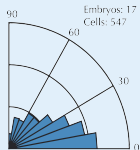
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Stretched Cells

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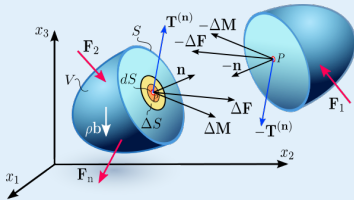


Division Angles

Align with stretch

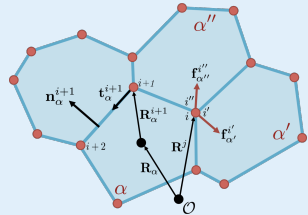
Modelling Approaches

Continuum mechanics



Capture tissue-level response to deformations.
– Bulk and shear modulus.

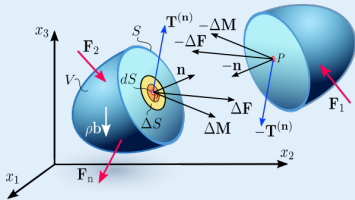
Discrete (vertex models)



Built from cell-level description.
Easy access to complex behaviours
e.g. remodelling.

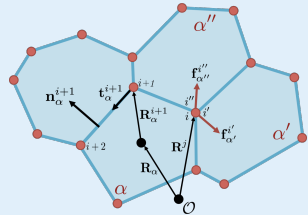
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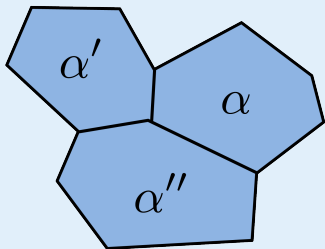
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The Mechanical Energy of a Cell

$$\tilde{U}_\alpha = \frac{\tilde{K}}{2} (\tilde{A}_\alpha - \tilde{A}_0)^2 + \frac{\tilde{\Gamma}}{2} (\tilde{L}_\alpha - \tilde{L}_0)^2$$



\tilde{A}_α = Area of cell α

\tilde{L}_α = Perimeter of cell α

\tilde{K} = Bulk stiffness

\tilde{A}_0 = Preferred area

\tilde{L}_0 = Preferred Perimeter

$\tilde{\Gamma}$ = Contractility

Farhadifar et al. (2007) > 600 citations!

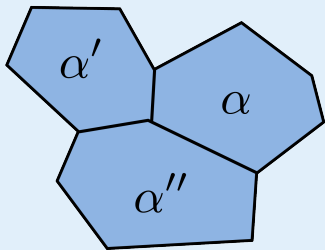
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Nondimensionalise:

$$A_\alpha = \frac{\tilde{A}_\alpha}{\tilde{A}_0}$$
$$L_\alpha = \frac{\tilde{L}_\alpha}{\sqrt{\tilde{A}_0}}$$

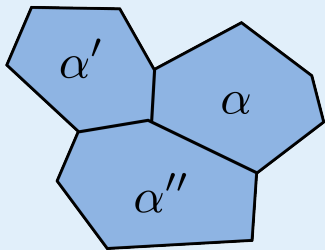
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The Mechanical Energy of a Cell

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A_{α} = Area of cell α

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L_0 = Preferred perimeter ($= -\frac{\Lambda}{2\Gamma}$)

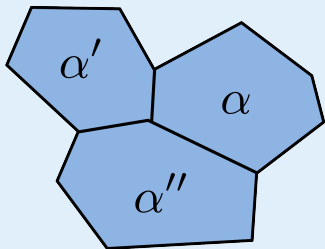
Λ = Line tension of cell edge

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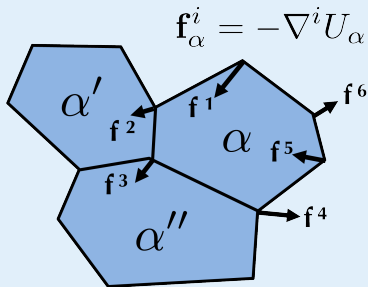
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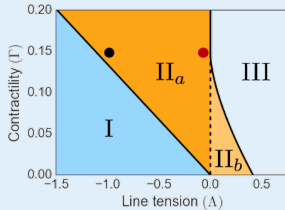
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Parameter Selection

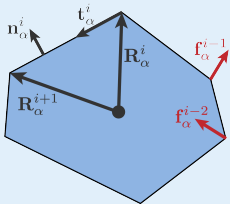


$$(\Lambda, \Gamma) = (-0.01, 0.15) \quad (\Lambda, \Gamma) = (-0.1, 0.15)$$



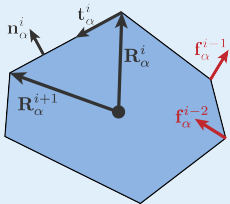
From Force to Stress

$$U_\alpha = \frac{1}{2} (A_\alpha - 1)^2 + \frac{\Gamma}{2} (L_\alpha - L_0)^2$$



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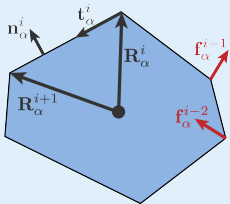
Define pressure and tension

$$P_\alpha = A_\alpha - 1$$

$$T_\alpha = \Gamma(L_\alpha - L_0)$$

From Force to Stress

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Elastic force

$$\begin{aligned} \mathbf{f}_\alpha^i &= \nabla^i U_\alpha \\ &= -\frac{1}{2} P_\alpha (\mathbf{n}_\alpha^i + \mathbf{n}_\alpha^{i-1}) + T_\alpha (\mathbf{t}_\alpha^i - \mathbf{t}_\alpha^{i-1}) \end{aligned}$$

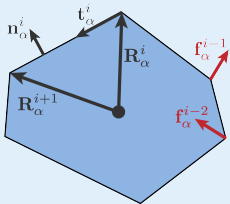
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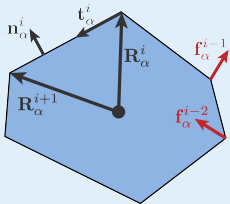
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Stress satisfies

$$\boldsymbol{\sigma} = \nabla \cdot (\mathbf{R} \otimes \boldsymbol{\sigma})$$

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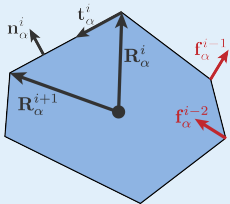
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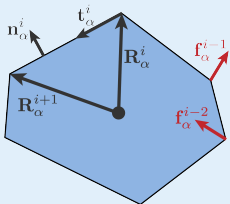
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From Force to Stress

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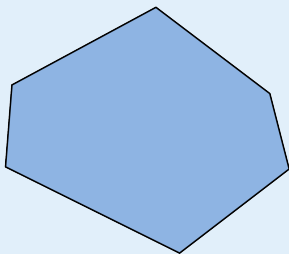
Motivating the definition

(Batchelor, 1970)

$$A_\alpha \boldsymbol{\sigma}_\alpha = \sum_{i=0}^{Z_\alpha-1} \mathbf{R}_\alpha^i \otimes \mathbf{f}_\alpha^i$$

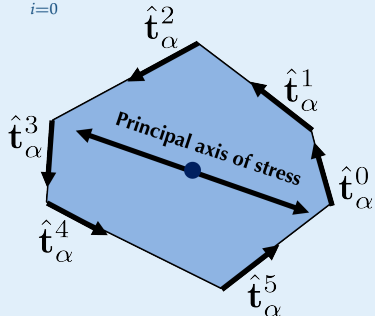
The Cell-Level Stress Tensor

$$\sigma_{\alpha} = -P_{\alpha}^{\text{eff}} \mathbf{1} + T_{\alpha} \mathbf{J}_{\alpha}$$



The Cell-Level Stress Tensor

$$Q = \frac{1}{L} \sum_{i=0}^{Z_\alpha-1} l_\alpha^i \hat{\mathbf{t}}_\alpha^i \otimes \hat{\mathbf{t}}_\alpha^i$$



$$\sigma_\alpha = -P_\alpha^{\text{eff}} \mathbf{1} + T_\alpha \mathbf{J}_\alpha$$

Tension $T_\alpha = \Gamma(L_\alpha - L_0)$

Deviatoric stress

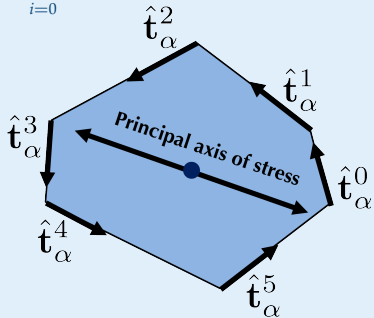
$$\mathbf{J}_\alpha = \frac{L_\alpha}{A_\alpha} \left(\frac{1}{2} \mathbf{1} - Q \right)$$

The Cell-Level Stress Tensor

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Deviatoric stress

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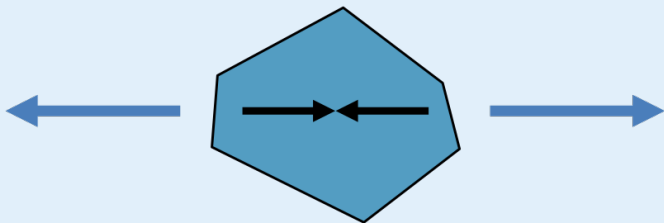
Isotropic stress

$$P_\alpha^{\text{eff}} = A_\alpha - 1 + \frac{T_\alpha L_\alpha}{2A_\alpha}$$

The Cell-Level Stress Tensor

- ▶ Cell principally under tension

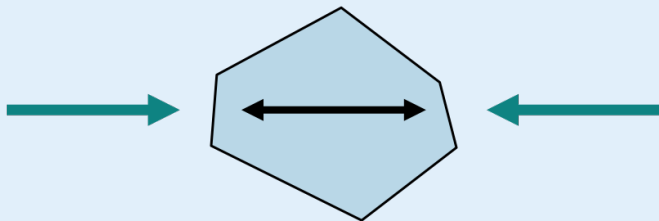
$$P_{\alpha}^{\text{eff}} > 0$$



The Cell-Level Stress Tensor

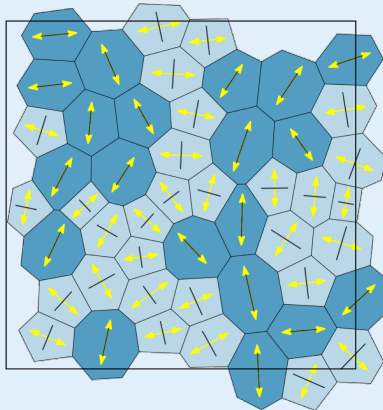
- ▶ Cell principally under compression

$$P_{\alpha}^{\text{eff}} < 0$$



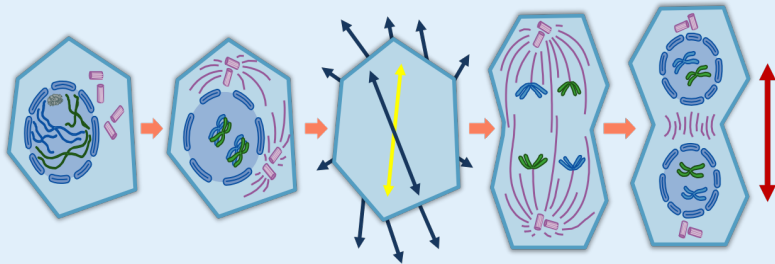
Cell-Level Stress and Shape Align

The principal axes of stress and shape align exactly.



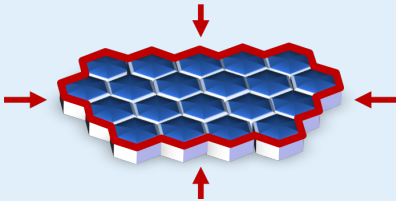
The stress and shape tensors commute and so share eigenbases.

Cell-Level Stress and Shape Align



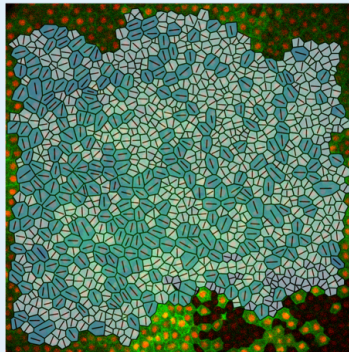
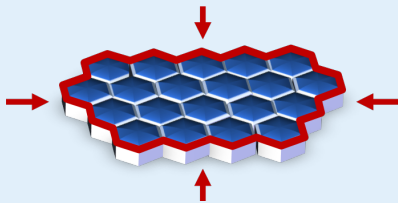
Local to Global Stress

$$\sigma^{\mathcal{M}} = \frac{1}{A^{\mathcal{M}}} \sum_{\alpha}^{N_c} A_{\alpha} \sigma_{\alpha}$$



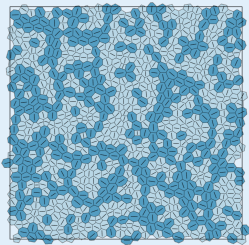
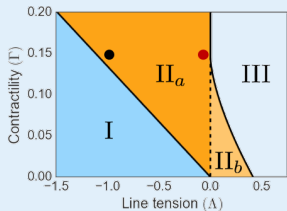
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Heterogeneity of Stress

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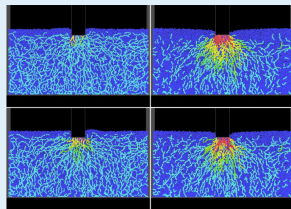
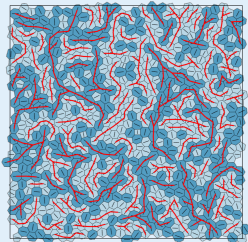
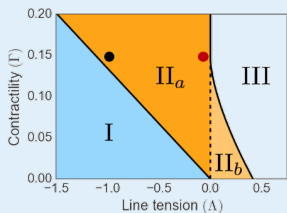


$$(\Lambda, \Gamma) = (-0.01, 0.15)$$



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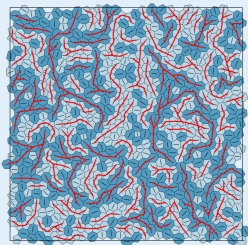
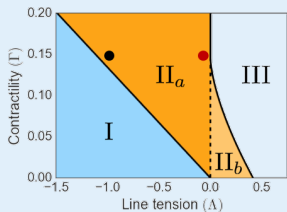


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Heterogeneity of Stress

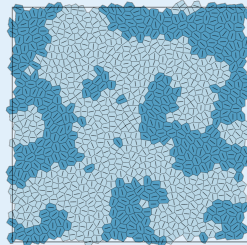
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$$(\Delta, \Gamma) = (-0.01, 0.15)$$



Lengthscales diverge

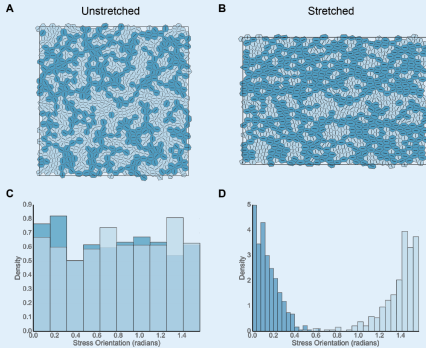


$$(\Delta, \Gamma) = (-0.1, 0.15)$$

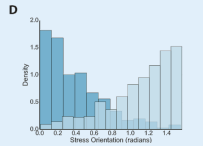
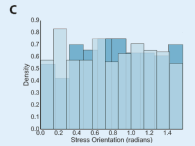
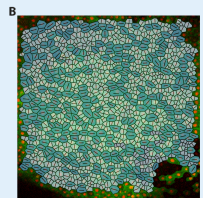
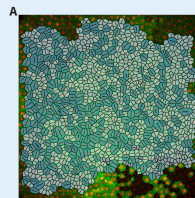
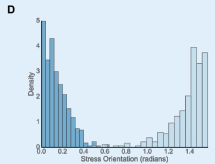
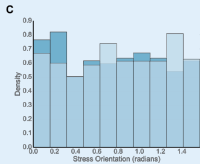
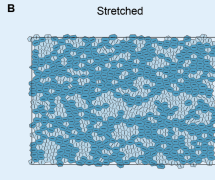
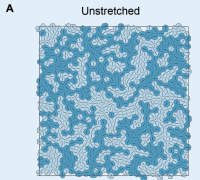


Deformation Promotes Organisation

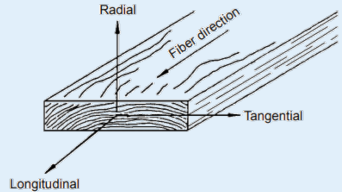
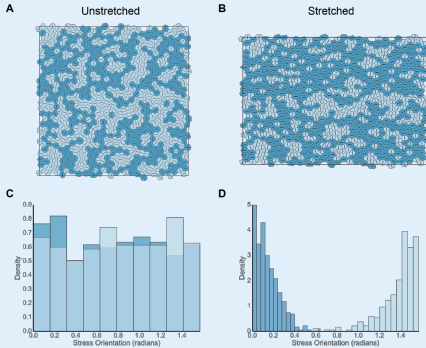
Small-on-Large Deformations Reveal Anisotropic Elasticity



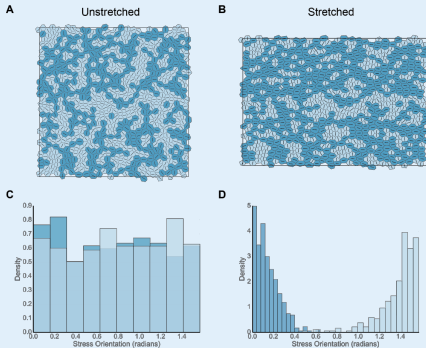
Small-on-Large Deformations Reveal Anisotropic Elasticity



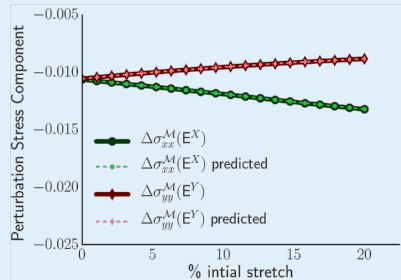
Small-on-Large Deformations Reveal Anisotropic Elasticity



Small-on-Large Deformations Reveal Anisotropic Elasticity



Apply strain in x : $E^x \dots$ and in y : E^y



Small-on-Large Deformations Reveal Anisotropic Elasticity

- ▶ Take pre-stressed base state, $\sigma^{\mathcal{M}}$
- ▶ Impose homogenous strain, E
- ▶ Position vectors transform as

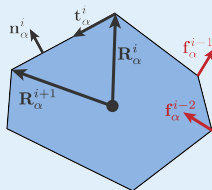
$$\mathbf{R}_\alpha^i \rightarrow \mathbf{R}_\alpha^i + E \cdot \mathbf{R}_\alpha^i \quad (1)$$

- ▶ To linear order,

$$\sigma^{\mathcal{M}} \rightarrow \sigma^{\mathcal{M}} + \Delta\sigma^{\mathcal{M}}$$

Expand stress,

$$\sigma^{\mathcal{M}}(\{\mathbf{R}_\alpha^i\}) \rightarrow \sigma^{\mathcal{M}}(\{\mathbf{R}_\alpha^i + E \cdot \mathbf{R}_\alpha^i\})$$



Small-on-Large Deformations Reveal Anisotropic Elasticity

- ▶ Take pre-stressed base state, $\sigma^{\mathcal{M}}$
- ▶ Impose homogenous strain, E
- ▶ Position vectors transform as

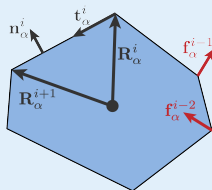
$$\mathbf{R}_{\alpha}^i \rightarrow \mathbf{R}_{\alpha}^i + E \cdot \mathbf{R}_{\alpha}^i \quad (1)$$

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Expand stress,

$$\sigma^{\mathcal{M}}(\{\mathbf{R}_{\alpha}^i\}) \rightarrow \sigma^{\mathcal{M}}(\{\mathbf{R}_{\alpha}^i + E \cdot \mathbf{R}_{\alpha}^i\})$$



Tangents: $\mathbf{t} = \mathbf{R}^{i+1} - \mathbf{R}^i$, and using (1):

$$\mathbf{t}^i + \Delta\mathbf{t}^i = \mathbf{R}^{i+1} - \mathbf{R}^i + E \cdot (\mathbf{R}^{i+1} - \mathbf{R}^i),$$

such that $\Delta\mathbf{t}^i = E \cdot \mathbf{t}^i$

Then lengths: $l^i = (\mathbf{t}^i \cdot \mathbf{t}^i)^{\frac{1}{2}} \dots$

Small-on-Large Deformations Reveal Anisotropic Elasticity

- ▶ Take pre-stressed base state, $\sigma^{\mathcal{M}}$
- ▶ Impose homogenous strain, E
- ▶ Position vectors transform as

$$\mathbf{R}_\alpha^i \rightarrow \mathbf{R}_\alpha^i + E \cdot \mathbf{R}_\alpha^i \quad (1)$$

- ▶ To linear order,

$$\sigma^{\mathcal{M}} \rightarrow \sigma^{\mathcal{M}} + \Delta\sigma^{\mathcal{M}}$$

Expand stress,

$$\sigma^{\mathcal{M}}(\{\mathbf{R}_\alpha^i\}) \rightarrow \sigma^{\mathcal{M}}(\{\mathbf{R}_\alpha^i + E \cdot \mathbf{R}_\alpha^i\})$$

Hooke's Law:

$$\Delta\sigma^{\mathcal{M}} = C : E$$

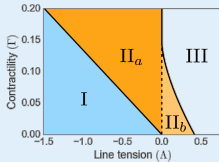
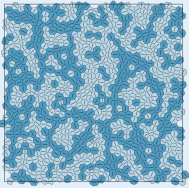
giving the stiffness tensor

$$C = \frac{1}{A^{\mathcal{M}}} \sum_{\alpha}^{N_c} [A_{\alpha}^2 \mathbf{I} \otimes \mathbf{I} + \Gamma L_{\alpha}^2 Q_{\alpha} \otimes Q_{\alpha} + L_{\alpha} T_{\alpha} (B_{\alpha} - Q_{\alpha} \otimes \mathbf{I})]$$

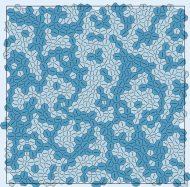
where

$$\begin{aligned} B_{\alpha} : E &= \frac{1}{L_{\alpha}} \sum_{i=0}^{N_v-1} l_{\alpha}^i [\hat{\mathbf{t}}_{\alpha}^i \otimes (E \cdot \hat{\mathbf{t}}_{\alpha}^i) \\ &= (E \cdot \hat{\mathbf{t}}_{\alpha}^i) \otimes \hat{\mathbf{t}}_{\alpha}^i - \hat{\mathbf{t}}_{\alpha}^i \otimes \hat{\mathbf{t}}_{\alpha}^i (\hat{\mathbf{t}}_{\alpha}^i \cdot E \cdot \hat{\mathbf{t}}_{\alpha}^i) \end{aligned}$$

Elastic Moduli for Isotropic Tissues

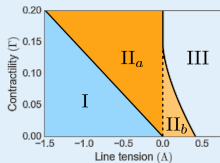
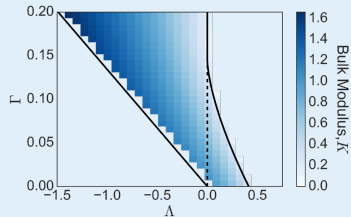


Elastic Moduli for Isotropic Tissues

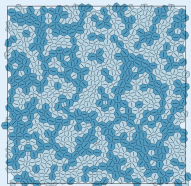


Bulk modulus

$$K = \frac{1}{2A\mathcal{M}} \sum_{\alpha=1}^{N_c} 2A_{\alpha}^2 + \frac{1}{2}\Gamma L_0 L_{\alpha}$$



Elastic Moduli for Isotropic Tissues

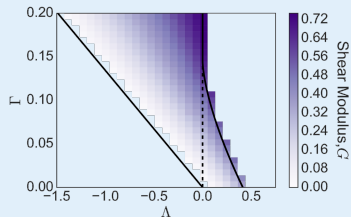
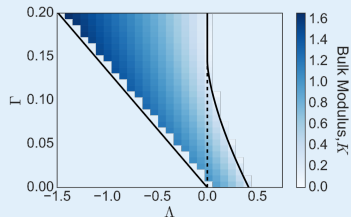
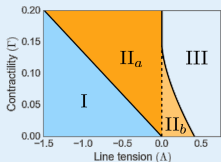


Bulk modulus

$$K = \frac{1}{2A^{\mathcal{M}}} \sum_{\alpha=1}^{N_c} 2A_{\alpha}^2 + \frac{1}{2}\Gamma L_0 L_{\alpha}$$

Shear modulus

$$G = \frac{3}{8A^{\mathcal{M}}} \sum_{\alpha=1}^{N_c} \Gamma L_{\alpha} (L_{\alpha} - L_0)$$



Murisic et al. (2015)

Understanding Forces in Morphogenesis

The Research Group

Sarah Woolner



Oliver Jensen

